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## (54) Hydrophilic contact lens coating

(57) The present invention provides a contact lens comprising an optically clear, transparent body having a lens surface, said lens surface defining a polymeric material carrying an ionic charge, a thin layer of a polyelectrolyte complex coating said lens surface and electrostatically bound thereto, said coating comprising an ionic polymer and said polymer forming a hydrogel at the surface which absorbs water, has good water retention and is compatible with the physiological structure of the eye.

The present invention also provides a solution and a method of treating contact lenses with the ionic polymer.

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#### **SPECIFICATION**

## Hydrophilic contact lens coating

5 The present invention is concerned with contact lenses, solutions for treating contact lens surfaces and a method of Coating Contact Lenses.

It has long been known in the art that a contact lens must have surfaces that have a certain degree of hydrophilicity in order to be wet by tears thus providing unblurred vision.

Soft, hydrophilic contact lens, in addition to being wettable, provide comfort to the wearer but lack the ability to correct visual deficiencies such as astigmatism since they tend to confirm to the shape of the corneal surface.

Often hydrophilic monomers can be added to a mixture of comonomers in the formation of contact lenses so that upon polymerization optically clear contact lenses result which have a certain degree of hydrophilicity. As the hydrophilic monomer content increases where it is added directly to the lens composition, the physical characteristics of the lenses are affected by the increased hydration propensity of the polymeric composition.

In some cases it has been known to treat a formed contact lens with a polymerizable hydrophilic monomer to form a surface coating of hydrophilic polymer grafted to an otherwise hydrophobic polymer surface.

Although effective, this method of increasing the hydrophilic character of the lens surface can suffer from involved and difficult manufacturing procedures.

Present rigid and soft contact lenses sometimes retain water on their surfaces through secondary chemical bonding and as a consequence only a very thin layer of water molecules is present between the eye and the contact lens.

contact lens.

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dryness between eye blinks. State of the art technology teaches that a water soluble neutral polymer may be

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applied to the surfaces of a hard contact lens to provide a "cushion" layer between the lens and the eye

which is equated with increased wettability as well as wearer comfort and tolerance.

Dissipation of the "cushion" layer occurs rapidly in most prior art constructions, since there is little specific interaction between the mobile polymer in this layer and the lens surface. As a result the wearer begins to feel discomfort and must recoat the lens surfaces.

It is an object of this invention to provide a hard or soft synthetic polymer contact lens whose surface carries a thin layer of polyelectrolyte complex coating the lens surface and electrostatically bound thereto.

It is another object of this invention to provide a method of rendering a contact lens that has an ionic surface more compatible with the eye by immersing the lens in a solution of an oppositely charged ionic polymer to form a thin polyelectrolyte complex on the lens surface, which complex increases its hydrophilic on a greater period of time relative to an untreated surface and which reduces the tendency for mucoproteins, a normal constituent of lacrimal tears, to adhere to a lens surface.

The layer or coating comprises a polyelectrolyte complex which is formed by reaction of an ionic lens surface with an oppositely charged ionic polymer, and this complex forms a hydrogel at the lens surface which absorbs water, has good water retention, and is compatible with the physiological structures of the eye. A durable "cushion" is formed which provides long lasting comfort to the eye.

In the preferred embodiment, the lens is an oxygen permeable hard lens which carries an ionic charge or has the potential of having an ionic charge. Preferably the lens coating is formed by merely immersing the lens in a solution which consists essentially of an ionic polymer dissolved in a water solution or a water solution containing soluble organic components comprising from 0.001 to 10% by weight of the solution. The ionic polymer can be any ionic polymer compatible with the eye and which does not cause eye irritation yet which forms a hydrogel and which is electrostatically bound to the surface of the contact lens.

It is a feature of this invention that thin coatings of from 20 to 2,500 Angstroms are formed, which coatings not only increase the compatibility of contact lens with the eye but also add a cushioning effect between the lens and the eye. Such coatings can avoid problems of punctate staining and further enhance the ability of the contact lens to be worn in the eye for periods up to 24 hours or more.

Depending on the concentration of ionic sites on the lens surface and the concentration of oppositely charged ionic polymer with which the surface is reacted, either wetting, soaking, or lubricating solutions can be prepared to provide optimal wearer comfortability. In addition, if cleaning agents are mixed with the ionic polymer solution, mucus, dirt and other unwanted deposits can be removed from the resulting

polyelectrolyte complex surface.

Soft and hard synthetic polymer contact lens materials are normally prepared from neutral monomers and/or polymers. In this invention both soft and hard contact lens materials are prepared in such a manner that ionic sites are present on the lens surface, such sites can be reacted with a lens solution containing an oppositely charged, hydrophilic polymer. If the surface of the lens is considered polyanionic, the surface can oppositely charged, hydrophilic polycation with the resulting formation of a hydrophilic polyelectrolyte then be reacted with a hydrophilic polycation with the resulting formation of a hydrophilic polyelectrolyte complexes have an equal amount of cations and anions, each obtained from a different source. In addition, these overall electrically neutral complexes exist as ionically cross-linked hydrogels that are effective in retaining water of hydration. In this invention, a surface coating of polyelectrolyte complex is achieved on a lens surface. A soft contact lens prepared entirely from a

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polyelectrolyte complex is known but would not have the desired properties of lenses preferred in accordance with this invention. In the present invention, it is possible that the reaction of ionic sites on a polymer surface, or potential ionic sites, with concommitant release of a low molecular weight electrolyte such as sodium chloride, hydrogen chloride, sodium sulfate, sodium methyl sulfate or any other related 5 electrolyte could give rise to a monolayer coating of polyelectrolyte complex.

Polyelectrolyte complexes, although highly hydrophilic, are water-insoluble and can be dissolved with some difficulty usually by a ternary solvent system incorporating water, a water-soluble organic compound, and a low molecular weight electrolyte. This solubility behavior implies that in the present invention the polyelectrolyte complex treated surface is very difficult to dissolve and separate from the lens surface by the 10 aqueous fluids of the eye, although this surface coating conceivably could be eroded by mechanical action in 10 the eye during wear. Should dissipation of the polyelectrolyte complex from the lens surface occur, it can readily be replaced by retreatment of the lens with the appropriate oppositely charged polyion solution.

The polyelectrolyte complex on the lens surface can be achieved by several means. If an anionic surface is desired, this can be accomplished by incorporation into the lens formulation of any monomer or monomers 15 from the acrylate or methacrylate salt group, a vinyl sulfonate salt, an allyl or methallyl sulfonate or sulfate salt, a styrene sulfonate salt, an acryloyloxy ethyl or methacryloyloxyethyl sulfate salt, a substituted acrylamido, or methacrylamido sulfonate salt or from related phosphonate, phosphate and phosphite salts of polymerizable monomers. Alternatively, a potentially anionic surface can be generated for subsequent treatment with a polycation followed by elimination of a low molecular weight acid (such as hydrogen 20 chloride) or by subsequent treatment with a neutral basic polymer resulting in an acid-base neutralization reaction. Such anionic monomers include compounds such as acrylic and methacrylic acid, vinyl-sulfonic acid, allyl or methallyl sulfonic or sulfuric acid, styrene sulfonic acid, an acrylamido or methacrylamido sulfonic acid, or a polymerisable phosphonic or phosphoric acid.

If a cationic surface is desired, this is accomplished by incorporation into the lens formulation of any 25 quaternary or protonated monomer or monomers from the acrylate or methacrylate salt group, a vinylpyridinium salt, a vinylimidazolium salt, a vinylimidazolinium salt, a vinylthiazolium salt, a vinylbenzylammonium salt, a diallyldialkylammonium salt, or a related alkylated or protonated polymerizable sulfonium or phosphonium salt. Alternatively, a potentially cationic surface can be generated for subsequent treatment with a polyacid resulting in an acid-base neutralization reaction. Such potentially cationic 30 monomers include compounds such as a dialkylaminoethyl acrylate or methacrylate, a vinylpyridine, a vinylimidazole, a vinylbenzyl amine, a vinyl alkyl ether or sulfide, or a polymerizable vinyl phosphine.

It is also possible to generate an ionic charge on the lens surface by chemically or electrically modifying a neutral monomeric repeat unit to one that is chargd. For example, an anionic surface can be obtained by treating a polyester material, such as polymethylmethacrylate, with an aqueous base, such as sodium 35 hydroxide, to yield sodium methacrylate units on the lens surface. Alternatively, a polyester material can be hydrolyzed with an acid to yield methacrylic acid units on the lens surface which function as potential anionic sites. Similarly, a cationic surface can be obtained by alkylating or protonating neucleophilic amine, sulfide or phosphine units on the lens surface.

Virtually all hard and soft contact lens materials presently disclosed are electrically neutral polymers or 40 copolymers. Such materials can be modified to include ionic surface groups. One general method for all types of lenses would include treatment of the surface with high energy irradiation in the presence of air to generate ionic surface groups, see A. Chaprio Radiation Chemistry of Polymeric Systems, Vol. XV, Interscience, New York, 1962, and F.A. Makhlis, Radiation Physics and Chemistry of Polymers, Wiley and Sons, New York, 1975.

Another method would include modification of polymeric lenses formulations through incorporation of ionic (or potentially ionic) monomers. Polymethyl methacrylate, which is currently the material of choice in the hard lens area, is amenable to such modification. Examples of this approach include the copolymerization of either acrylic acid, methacrylic acid or dimethylaminoethyl methacrylate to provide a polymethyl methacrylate lens with ionic groups on the surface.

Another example would include the modification of oxygen permeable lens formulations such as those in U.S. Patent 3,808,178. These formulations are copolymers of methyl methacrylate with a siloxanylalkyl ester of methacrylic acid and can be modified through the addition of either acrylic acid, methacrylic acid or dimethylaminoethyl methacrylate.

In a similar fashion the monomers acrylic acid, methacrylic acid or dimethylaminoethyl methacrylate 55 could be employed as co-reactants with hydroxyethyl methacrylate to produce a material that is suitable for soft contact lenses which, in addition, provides an ionic surface.

Cellulosic polymers such as cellulose acetate butyrate have found use as contact lenses materials which exhibit moderate oxygen permeability. Polymers of this type contain residual cellulose alcohol functionalities which can be utilized as modification sites. Reaction of sodium chloroacetate with the alcohol 60 functionalities will result in pendent carboxylate groups along the polymer chain. Contact lens produced from this modified CAB material would be inherently wettable with an ionic surface receptive to

polyelectrolyte complex formation. The synthetic resin lens preferably has a total ionic charge of from 0.001% to 10%. Thus from 0.001% to 10% of the surface area is charged and the charge density often is about 5%.

The lens solutions of this invention are in all cases USP sterile, preferably water solutions containing

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ingrecients common to lens solutions and which carry from 0.001 to 10% by weight of a water soluble ionic polymer or polymers such as:

	polymer or polymers such as:	
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	Cationic	5
5	to the second conditioners of:	
•	N,n-dimethylaminoethyl acrylate and methacrylate  N,n-dimethylaminoethyl acrylate and methacrylate	
	2-methacryloyloxyethyltrimethylamillomani amovas and	
	- 4 - 40 - ashvi-E-vinvinvinvinuini cilionide and moury	10
_	2-,4-, and 2-methyl-5-viny,pythylamine  N-(3-methacrylamidopropyl)-N,N-dimethylamine  N-(3-methacrylamidopropyl)-N,N-dimethylammonium chloride	
1	N-(3-methacrylamidopropyl)-N,N,N-trimethylammonium chloride N-(3-methacrylamidopropyl)-N,N,N-trimethylammonium chloride	
	N-(3-methacrylantuoptopy) visionidazole	
	1-vinyl- and 2-methyl-1-vinylimidazole 1-vinyl- and 2-methyl-1-vinylimidazolium chloride and methylsulfate 1-vinyl- and 2-methyl-1-vinylimidazolium chloride	
	1-vinyl- and 2-methyl-1-vinylihidazonih olivorih vinyl- and 2-methyl- an	. 15
	N-(3-acrylamido-3-inetryloddy), at a state ortholography chloride	
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	it - it dimethylammentum chieffee and mean to the	
	vinylbenzyltrimethylammonium chloride	00
	cationic starch	20
	O cationic cellulose	
•	ionene polymers	
	Anionic sodium carboxymethylcellulose	
	sodium carboxymethylbydroxyethylcellulose	25
	sodium carooxymeethyladoxy	
	25 sodium carboxymethylstarch	
	sodium carboxymethyldydroxyethylstarch sodium carboxymethyldydroxyethylstarch	
	hydrolyzed polyacrylamide and polyacrylonitrile	
	homopolymers and copolymers of.	30
	panylic and methacrylic acids	<b></b>
	30 Sodium acrylate and methacrylate	
	vinylsulfonic acid	
	sodium vinylfulfonate	
	n-styrenesulfonic acid	35
	and the prepared sufforate	35
	tenterothyletilfonic acid	-
	a methodylovicy-7-hydroxypropyradiomedata	
	2-acrylamido-2-methylpropanesulfonic acid	
	allulantionic acid	
	2-phosphatoethyl methacrylate  Other additives to the soaking lens solutions of this invention include conventional lens solution cleaning  Other additives to the soaking lens solutions of this invention include conventional lens solution cleaning	40
	2-pnospiratoethyr measurements of this invention include conventional tens solutions of the solution in the solu	
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	and soaking solution additives. Preservatives such as benzyalkonium chloride, surjustically alcohol, acid (EDTA), mercurials and chlorobutanol can be used. Wetting agents such as polyvinyl alcohol, acid (EDTA), mercurials and chlorobutanol can be used. Lubricating agents such as the wetting	
	and soaking solution account and chlorobutanol can be used. Wetting agents such as polyviny, acid (EDTA), mercurials and chlorobutanol can be used. Lubricating agents such as the wetting hydroxypropyl methylcellulose and methyl cellulose can be used. Soaking and cleaning agents such as neutral hydroxypropyl methylcellulose and methyl cellulose can be used. Soaking and cleaning agents such as neutral hydroxypropyl methylcellulose and methyl cellulose can be used.	ł
	hydroxypropyl methylcellulose and the concentrations can be used. Soaking and cleaning agents such as housed	45
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	Other conventional buffers, biocides and viscosity modifiers may also be used. The additives of body pH wide range of concentrations as known in the art. Preferably the pH of the solutions are as near to body pH wide range of concentrations as known in the art. Preferably the pH of the solution can also be	dS
	possible and always in the range of pH 6-8.  While it is preferred to merely soak the lens in the solution at room temperature, the solution can also be  While it is preferred to merely soak the lens in the solution at room temperature, the solution can also be	50
	While it is preferred to merely soak the lens in the solution at room temperature.	50
	to all cases it is preferred to form a coating of no more than 2,300 A obtaining linked polymer that	
	In all cases it is preferred to form a coating of no more than 2,500 A over the left state of the polymer that hydrogel. The hydrogel formed by the polyelectrolyte complex is an ionically cross linked polymer that hydrogel. The hydrogel formed by the polyelectrolyte complex is an ionically cross linked polymer that hydrogel. The hydrogel formed by the polyelectrolyte complex is an ionically cross linked polymer that hydrogel. The lenses tend to be absorbs large amounts of water and at least 10% of its own weight of water. The lenses tend to be absorbs large amounts of water and at least 10% of its own weight of water.	
	absorbs large amounts of water and at least 10% periods of time. non-irrating to the eye and can be worn for long periods of time.  55 Specific examples of this invention are given below but are not meant in any way to limit this invention.	55
•	non-irrating to the eye of this invention are given below but are not meant in any way to	
	55 Specific examples of this invention and also from a	
	EXAMPLE I  Hard polymeric test samples were prepared from methyl-methacrylate (MMA) and also from a  Hard polymeric test samples were prepared (MMA) and methacrylic acid (MA). A minor amount of	
	Hard polymeric test samples were methacrylate (MMA) and methacrylic acid (MA). A million and acceptaining age	nt.
	and a most mixture of the formulations as a cross minimum of	60
		s.
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	tubes, stoppered, degassed, then filled with nitrogen. The test tubes were placed in a without tubes, stoppered, degassed, then filled with nitrogen. The test tubes were for an additional three days allowed to polymerize for two days. The tubes were then placed in a 60°C oven for an additional three days allowed to polymerize for two days. The tubes were then placed to	es 65
	allowed to polymerize for two days. The tubes were then placed in a 60 C over 161 days allowed to polymerize for two days. The tubes were then subjected to after which the polymerized rods were removed from the tubes. The rods were then subjected to after which the polymerization process.	
	allowed to polymerize for two days. The removed from the tubes. The rods were then subjected to after which the polymerized rods were removed from the tubes. The rods were then subjected to after which the polymerization processor which the polymerization processor conditioning for approximately fifteen hours at 100°C under vacuum to complete the polymerization processor conditioning for approximately fifteen hours at 100°C under vacuum to complete the polymerization processor.	

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and relieve any mechanical stresses present. Test specimens, in the form of 3/16" by 1/2" discs, were machined from the conditioned rods. The flat machined surfaces of the discs were then highly polished to provide an appropriate surface for contact angle measurements.

Contact angles were determined on hydrated specimens after immersed in H<sub>2</sub>O for 2 days with the values 5 representing the advancing water droplet angle on the polished surface. Lower angles are indicative of more wettable materials which can be attributed to a more polar surface either as a result of the chemical groups present or the presence of bound water molecules.

The significantly lower contact angle produced by surface treatment "B" clearly illustrates the embodiment of this invention. The cationic hydroxyethylcellulose is ionically bound to the surface 10 carboxylate (anionic) groups producing a layer of polyelectrolyte complex which contains bound water.

TABLE I

	Composition (wt. percent	n reagent)			Surface Treatment	Advancing Angle in degrees	.15
15	MMA	MA	TEGDM	AZO			
20	98:8 93.8 93.8 93.8	5 5	1.0 1.0 1.0 1.0	0.2 0.2 0.2 0.2	none none A* B**	82-84 74-75 77-78 64-65	20

\*Treatment "A" was a five minute immersion in a sodium carbonate water solution (pH = 10.7) followed by a thorough rinse with distilled water.

25 \*\*Treatment "B" was initially identical to treatment "A" with a subsequent five minute immersion in a 0.1 weight percent cationic hydroxyethylcellulose (Union Carbide JR-125 resin) water solution at room temperature followed by a thorough rinse with distilled water.

Using the experimental procedures described in Example I hard polymeric test samples were prepared **EXAMPLE II** 30 from methyl methacrylate (MMA), methacryloyloxypropyl tris(trimethylsilyl) siloxane (TRIS) and methacrylic 30 acid (MA). A minor amount of tetraethylene glycol dimethacrylate (TEGDM) was incorporated as a crosslinking agnt. The free radical initiator 2,2'-azobisisobutyro-nitrile (AIBN) was utilized to effect polymerization. The concentration of reagents employed, surface treatments and contact angle values are presented in Table II. this particular formulation was chosen as typical of those presently utilized in the 35 35 production of hard, oxygen permeable contact lenses.

TABLE II

40	(wt	Composition percent reagent)	40
45	MMA TRIS MA TEGDM AZO	59.4 34.6 4.9 0.9 0.2	45
Surface Treatment	Advar	ncing angle in degrees	50
50 none "A" "B"	80-82 82-83 77-78 78-79		55
"C"* 55 *Treatment "C" was initially weight percent polyvinylbe	,	ith a subsequent five minute immer oride water solution followed by a th	sion in a 0.1

with distilled water. Using the experimental procedures described in Example I hard polymeric test samples were prepared from methyl methacrylate (MMA), methacryloyloxypropyl tris(trimethylsilyl) siloxane (TRIS) and dimethylaminoethyl methacrylate (DMAEM). A minor amount of tetraethylene glycol dimethacrylate (TEGDM) was incorporated as a crosslinking agent. The free radical initiator 2,2'-azobisisobutyronitrile (AIBN) was utilized to effect polymerization. The concentration of reagents employed, surface treatments and contact angle

65 values are presented in Table III. This particular composition was chosen as typical of a material which could

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be utilized in the production of highly oxygen permeable, hard contact lenses.

This example illustrates the incorporation of a cationic monomer in the polymer formulation which is receptive to treatment with an anionic polymer to form a surface layer f poly-electrolyte complex. This behavior demonstrates the versatility of the present invention in that either an anionic (Examples I and II) or 5 a cationic (Example III) monomer may be incorporated into a polymeric formulation which is capable of forming a polyelectrolyte complex with a polyion of the opposite charge.

TABLE III

	Composition (wt. percent reagent)			10
10 .	MMA TRIS DMAEM	51.8 42.4 4.7		
_	TEGDM AZO	0.9 0.2		15
15	Advancing	angle in degrees		
Surface Treatment	83-84			
none	84-85	•. •		
"D"* "E"**	75-76			20
20 "F"***	77-78			

\*Treatment "D" was a five minute immersion in a hydrochloric acid solution (pH = 3.0) followed by a thorough rinse with distilled water.

\*\*Treatment "E" was a five minute immersion in a 0.1 weight percent polyacrylic acid water solution 25 followed by a thorough rinse with distilled water.

\*\*\*Treatment "F" was initially identical to treatment "D" with a subsequent five minute immersion in a 0.1 weight percent sodium polystyrenesulfonate water solution followed by a thorough rinse with distilled

In general, the polymeric material of the lens is preferably selected from the group comprising:

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40 where  $R_1 = H$ ,  $CH_3$ ,  $CH_2COOH$ ,  $CH_2COOCH_3$ , or  $CH_2COOC_6H_5$ , and  $R_2 = H$ , or  $C_1-C_{20}$  derivative of a monohydric alkanol, a C1-C3 derivative of dihydric and trihydric alkanols, or

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$$A - Si - A$$

$$CH_2)_a - Si - O - Si - (O)_a - D$$

$$A - Si - A$$

where "a" is an integer from one to three, "b" and "c" are integers from zero to two, "d" is an integer from 60 zero to one, A is selected from the class of methyl and phenyl groups, B is selected from the class of methyl or phenyl groups, C and D represent either no group (cyclic ring from "c" to "d") or methyl or phenyl groups.

The polymeric material can also consist essentially of:

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R<sub>1</sub> - S<sub>2</sub> - C 1 R<sub>2</sub>

10 where  $R_1$  and  $R_2$  are selected from H,  $CH_3$ ,  $C_2H_5$ ,  $C_3H_7$ ,  $C_6H_5$ , COOH,  $CH_2$ =CH- and -0- groups. In some cases, the polymeric material consists essentially of cellulose units having the formula:

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where  $R_1$ ,  $R_2$  and  $R_3$  are selected from H, derivatives of  $C_1$ - $C_{20}$  carboxylic acid,  $C_1$ - $C_{20}$  alkyl groups,  $C_1$  to  $C_3$  monohydric and dihydric alkanols, phenyl groups,  $CH_2COOH$ , and  $CH_2CH_2\bar{N}R_3$  groups wherein  $R_4$  = H,  $CH_3$ , 25 or  $C_2H_5$ .

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While specific polymers described can be used alone, they can also be used in combination with each other. For example, the lens composition can comprise a mixture of two or more different derivatives of acrylic or methacrylic acid. It is important that the ionic charge be present and that the polymer or polymer mixture provide good contact lens characteristics as known in the art such as optical clarity.

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Preferably the contact lenses have a lens surface which contain ionic sites which are complexed to oppositely charged polymer sites selected from the groups COOX, SO<sub>3</sub>X, and PO<sub>3</sub>X, wherein X = H or monovalent inorganic ion  $\bar{N}$  (R)<sub>3</sub> groups, wherein R = H, CH<sub>3</sub> or C<sub>2</sub>H<sub>5</sub> groups,  $\bar{S}(R')_2$ , wherein R' = H, CH<sub>3</sub>, or C<sub>2</sub>H<sub>5</sub> groups,  $\bar{P}(R'')_3$ , wherein R" = H, CH<sub>3</sub>, C<sub>2</sub>H<sub>5</sub> and phenyl groups, pridinium groups and imidazolium groups.

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35 What is claimed is:

#### CLAIMS

A contact lens comprising an optically clear, transparent body having a lens surface,
 said lens surface defining a polymeric material carrying an ionic charge,
 a thin layer of a polyelectrolyte complex coating said lens surface and electrostatically bound thereto,
 said coating comprising an ionic polymer and said polymer forming a hydrogel at the surface which
 absorbs water, has good water retention and is compatible with the physiological structure of the eye.
 A contact lens in accordance with claim 1 wherein said polymeric material is:

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where  $R_1 = H$ ,  $CH_3$ ,  $CH_2COOH$ ,  $CH_2COOCH_3$ , or  $CH_2COOC_6H_5$ , and  $R_2 = H$ , or  $C_1-C_{20}$  derivative of a monohydric alkanol, a  $C_1-C_3$  derivative of dihydric and trihydric alkanols, or

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$$\begin{array}{c|c}
B \\
\hline
A-Si-A \\
\hline
(CH_2)_{a} - Si-O-Si-(O)_{a} - D \\
\hline
A-Si-A \\
\hline
C
\end{array}$$
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where "a" is an integer from one to three, "b" and "c" are integers from zero to two, "d" is an integer from zero to one, A is selected from the class of methyl and phenyl groups, B is selected from the class of methyl 20 or phenyl groups, C and D represent either no group (cyclic ring from "c" to "d") or methyl or phenyl groups. 20

3. A contact lens in accordance with claim 1 and further comprising said polymeric material consisting essentially of

where R<sub>1</sub> and R<sub>2</sub> are selected from H, CH<sub>3</sub>, C<sub>2</sub>H<sub>5</sub>, C<sub>3</sub>H<sub>7</sub>, C<sub>6</sub>H<sub>5</sub>, COOH, CH<sub>2</sub>=CH- and -0- groups.

4. A contact lens in accordance with claim 1 and further comprising said polymeric material consisting

35 essentially of cellulose units having the formula

where  $R_1$ ,  $R_2$  and  $R_3$  are selected from H, derivatives of  $C_1$ - $C_{20}$  carboxylic acid,  $C_1$ - $C_{20}$  alkyl groups,  $C_1$  to  $C_3$  monohydric and dihydric alkanols, phenyl groups,  $C_1$ - $C_2$ - $C_3$ - $C_4$ - $C_5$ - $C_4$ - $C_5$ - $C_5$ - $C_6$ - $C_6$ - $C_6$ - $C_7$ - $C_8$ -

- CH<sub>3</sub>, or C<sub>2</sub>H<sub>5</sub>.

  5. A contact lens in accordance with claim 1 wherein said lens surface contains ionic sites which are complexed to oppositely charged polymer sites selected from the groups COOX, SO<sub>3</sub>X, and PO<sub>3</sub>X, wherein X = H or monovalent inorganic ion, N(R)<sub>3</sub> groups, wherein R = H, CH<sub>3</sub> or C<sub>2</sub>H<sub>5</sub> groups, S(R')<sub>2</sub>, wherein R' = H, CH<sub>3</sub>, or C<sub>2</sub>H<sub>5</sub> groups, P(R")<sub>3</sub>, wherein R" = H, CH<sub>3</sub>, C<sub>2</sub>H<sub>5</sub> and phenyl groups, pyridinium groups and imidazolium groups.
- imidazolium groups.

  55 6. A contact lens in accordance with claim 1 wherein said lens surface has a total ionic charge of from
  - 0.001% to 10%.
    7. A contact lens in accordance with claim 6 wherein said thin layer of polyelectrolyte complex coating has a thickness in the range of from 20 to 2,500 Angstroms.
- 8. A contact lens in accordance with claim 2 wherein said lens surface contains ionic sites which are 60 complexed to oppositely charged polymer sites selected from the groups COOX, SO<sub>3</sub>X, and PO<sub>3</sub>X, wherein X 60 = H or monovalent inorganic ion,  $\bar{N}(R')_3$  groups, wherein R = H, CH<sub>3</sub> or C<sub>2</sub>H<sub>5</sub> groups,  $\bar{S}$  (R')<sub>2</sub>, wherein R' = H, CH<sub>3</sub>, or C<sub>2</sub>H<sub>5</sub> groups,  $\bar{P}$  (R")<sub>3</sub>, wherein R" = H, CH<sub>3</sub>, C<sub>2</sub>H<sub>5</sub> and phenyl groups, pyridinium groups and imidazolium groups.
- 9. A contact lens in accordance with claim 3 wherein said lens surface contains ionic sites which are 65 complexed to oppositely charged polymer sites selected from the groups COOX, SO<sub>3</sub>X, and PO<sub>3</sub>X, wherein X 65

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<u>-</u>	= H or monovalent inorganic ion, $\tilde{N}(R)_3$ groups, wherein $R=H$ , $CH_3$ or $C_2H_5$ groups, $\tilde{S}(R')_2$ wherein $R'=H$ , $CH_3$ , or $C_2H_5$ groups, $\tilde{P}(R'')_3$ , wherein $R'=H$ , $CH_3$ , $C_2H_5$ and phenyl groups, pyridinium groups and
iı	midazolium groups.
	10. A contact lens in accordance with claim 4 wherein said lens surface contains ionic sites which are
5 0	complexed to appositely charged polymer sites selected from the groups COOX, SO <sub>3</sub> X, and PO <sub>3</sub> X, wherein
•	the state of the s

complexed to oppositely charged polymer sites selected from the groups COOX,  $SO_3X$ , and  $PO_3X$ , wherein = H or monovalent inorganic ion, $\tilde{N}(R)_3$  groups, wherein R = H,  $CH_3$  or  $C_2H_5$  groups,  $\tilde{P}(R')_2$ , wherein R' = H,  $CH_3$ , or  $C_2H_5$  groups,  $\tilde{P}(R')_3$ , wherein R' = H,  $CH_3$ ,  $C_2H_5$  and phenyl groups, pyridinium groups and imidazolium groups.

11. A contact lens in accordance with claim 7 wherein said lens surface contains ionic sites which are
10 complexed to oppositely charged polymer sites selected from the groups COOX, SO<sub>3</sub>X, and PO<sub>3</sub>X, wherein X
= H or monovalent inorganic ion, N(R)<sub>3</sub> groups, wherein R = H, CH<sub>3</sub> or C<sub>2</sub>H<sub>5</sub> groups, S(R')<sub>2</sub>, wherein R' = H,
CH<sub>3</sub>, or C<sub>2</sub>H<sub>5</sub> groups, P(R")<sub>3</sub>, wherein R" = H, CH<sub>3</sub>, C<sub>2</sub>H<sub>5</sub> and phenyl groups, pyridinium groups and imidazolium groups.

A lens solution for treating contact lens surfaces, said lens solution consisting essentially of an ionic
 polymer in water solution with said polymer being present in an amount of from 0.001 to 10% by weight of said solution,

said solution being sterile and having a physiologically acceptable pH.

13. A lens solution in accordance with the lens solution of claim 12 and further comprising lens cleaning and preserving additives.

20 14. A method of forming a polyelectrolyte complex coating on a polymeric lens, said method comprising,

wetting said lens surface with a wetting solution carrying an ionic polymer to form a thin layer of said polylectrolyte complex electrostatically bound to said surface,

said coating comprising an ionic polymer and said polymer forming a hydrogel at said surface which 25 absorbs water, has good water retention and is compatible with the physiological structure of the eyes.

15. Contact lenses according to claim 1, esubstantially as hereinbefore decribed and exemplified.15. A solution for treating contact lens surfaces, substantially as hereinbefore described and examflified.

17. A method according to claim 14 of forming a coating on a contact lens, substantially as hereinbefore described and exemflified.

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# XP-002103586

1/1 - (C) WPI / DERWENT

AN - 89-223299 ç31!

AP - JP860308716 861226

PR - JP860308716 861226

TI - Washing and preserving soln. for contact lens - contains water-soluble cationic polymer dissolved in saline soln. or pure water

IW - WASHING PRESERVE SOLUTION CONTACT LENS CONTAIN WATER SOLUBLE CATION POLYMER DISSOLVE SALINE SOLUTION PURE WATER

PA - (DAIL ) DAICEL CHEM IND LTD

PN - JP1158412 A 890621 DW8931 003pp

ORD - 1989-06-21

IC - C11D17/00; G02C7/04; G02C13/00

FS - CPI; GMPI

DC - A18 A96 D22 P81

AB - J01158412 Soln. contains water-soluble cationic polymer, which is dissolved in physiological saline soln. or pure water.

The cationic polymer of natural polysaccharide such as cellulose, starch, tamarind, etc. and their derivs. to which are added alkylene oxide or glycidol is used. Cationic polyvinyl pyrrolidone, cationic polyacrylic acid, etc. and their derivs. can be used. The mixts. of at least two kinds of cationic polymers can be used. The amt. of the cationic polymer to soln. is 0.01-5 wt.\*, pref. 0.01-2 wt.\*. The buffer agent and other additives can be used.

- USE/ADVANTAGE - Used for washing and preserving soln. for contact lens. The soln. has both functions for washing and preservation. It keeps hydrophilic property of the lens surface and suppresses the reproduction of bacteria. The addn. of germicide is not needed. (0/0)